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(54) **Antibacterial vascular prosthesis and surgical suture**

Antibakterielle Gefäßprothese und chirurgisches Nahtmaterial

Prothèse vasculaire et suture chirurgicale antibactérienne

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(56) References cited:  
**EP-A- 0 230 635** **EP-A- 0 328 421**  
**EP-A- 0 334 046** **EP-A- 0 448 840**  
**EP-A- 0 531 547** **WO-A-91/15251**  
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## Description

### FIELD OF THE INVENTION

**[0001]** The present invention relates to a vascular prosthesis suitable for use as a substitute for an artery, vein or the like and a surgical suture, and more particularly to a vascular prosthesis and a surgical suture, both, given with an antibacterial activity.

### BACKGROUND OF THE INVENTION

**[0002]** Vascular prostheses composed of a tubular porous body formed of a synthetic polymer such as polytetrafluoroethylene (hereinafter abbreviated as "PTFE") or polyester are widely used in repair of circulation or for internal shunts upon dialysis. However, such vascular prostheses involve a serious problem that they tend to be infected with bacteria. More specifically, the bacteria entered upon implantation of a vascular prosthesis, or the like are easy to proliferate on an artificial material such as the vascular prosthesis because an immune system, which is an innate protective system in the living body, is hard to normally and sufficiently operate in such circumstances. In addition, tissue cells and intracellular substances damaged or destroyed by grafting, or blood coagulation occurred in the damaged site provide suitable proliferative sites for the entered bacteria.

**[0003]** As methods for preventing the bacterial infection, for example, it has been conducted to sterilize a vascular prosthesis before its use, and to make a surgical field thoroughly sterile. However, the infection rate is considerably high as reported to be 1-5%. In order to treat an infectious disease, it is conducted to administer one or more antibiotics. By this method, however, it is difficult to topically exert their antibacterial effect on the site in which bacteria are grown. It has hence been only necessary to excise or remove the vascular prosthesis once it has become infected.

**[0004]** As methods for protecting a vascular prosthesis from bacterial infection, there have heretofore been proposed various methods in which an antibacterial activity is imparted to the vascular prosthesis itself. For example, there have been proposed (1) a vascular prosthesis obtained by applying or depositing a silver-antibiotic complex on a porous structure formed of PTFE or polyester [A. I. Benvenisty et al., J. Surgical Research, 44, 1-7 (1988)], and (2) a vascular prosthesis obtained by coating a PTFE or polyester material with a surfactant and then bonding an antibiotic to the surfactant by ionic bonding [W. B. Shue et al., J. Vascular Surgery, 8, 600-605 (1988)]. However, the amount of antibiotic is small and therefore it does not last until peripheral tissues, including the interior of the wall of the vascular prosthesis, have healed. A second problem is that the antibiotic and surfactant present in the wall and on the inner wall surface of the vascular prosthesis impair its

antithrombogenicity and histocompatibility.

**[0005]** In addition to the above methods, there have been proposed (3) methods in which a mixture of a biopolymer such as glucosaminoglycan-keratin or collagen and an antibiotic is applied onto the inner wall or outer surface of a vascular prosthesis [K. R. Sobinsky et al, Surgery, 100, 629-634 (1986), and M. D. Colburn et al, J. Vascular Surgery, 16, 651-660 (1992)]. According to these methods, the amount of the antibiotic to be combined can be increased, and the release rate of the antibiotic can be controlled. However, in addition to the second problem given in the preceding paragraph, the porous structure within the wall of the vascular prosthesis is filled with the biopolymer, so that living tissues cannot penetrate the outer and inner walls, and healing is not achieved.

**[0006]** EP-A-0328421 discloses infection-resistant medical devices, such as for example catheters, surgical sutures, wound dressing, arterial grafts, etc., made up of expanded polytetrafluoroethylene (PTFE) and coated with a porous biodegradable polymer (polylactic acid) containing an antibacterial substance (silver compounds, antibiotics).

### SUMMARY OF THE INVENTION

**[0007]** According to the present invention, a vascular prosthesis comprises a tubular porous body formed of a synthetic polymer and, wound around the body, a tube, fibre or sheet formed from a polymeric material and combined with an antibacterial substance, wherein the outer surface of the body is partially uncovered and the porosity of the prosthesis relative to that of the body is unimpaired.

**[0008]** Since the tube, fiber or sheet combined with the antibacterial substance is wound on the outer surface of the vascular prosthesis with a desired space, the porous structure of the vascular prosthesis is not impaired, and the functions of the vascular prosthesis, such as antithrombogenicity and histocompatibility, are not impeded. The antibacterial substance can be gradually released over a long period of time from the tube, fiber or sheet. The antibacterial substance gradually released in the vicinity of the outer surface of the vascular prosthesis inhibits the growth of bacteria attached to the vascular prosthesis over a long period of time.

### BRIEF DESCRIPTION OF THE DRAWING

**[0009]** FIG. 1 diagrammatically illustrates the amount of an antibacterial substance released with time from an antibacterial vascular prosthesis obtained in an example of the present invention.

## DETAILED DESCRIPTION OF THE INVENTION

Tubular porous body

[0010] In the present invention, a tubular porous body formed of a synthetic polymer is used as a vascular prosthesis. Examples of the synthetic polymer from which the vascular prosthesis is formed include polytetrafluoroethylene, polyester, polyurethane, polyethylene, polypropylene and polysiloxane.

[0011] No particular limitation is imposed on the process for producing the tubular porous bodies from these synthetic polymer materials. They may be produced in accordance with a process known per se in the art according to the material used. For example, a tubular porous body made of PTFE can be produced in accordance with the process described in Japanese Patent Publication No. 13560/1967. More specifically, a liquid lubricant is first mixed into unsintered PTFE powder, and the mixture is extruded through a ram extruder into a tubular form. The tube is stretched at least in its axial direction after removing liquid lubricant from the tube or without removing the liquid lubricant. Both ends of the tube are then fixed so as to prevent it from shrinking, and the tube is heated from both inner and outer sides thereof at 327°C which is a sintering temperature of PTFE, or higher, thereby obtaining a tubular PTFE porous body having a fine fibrous structure composed of fibers and knots joined to each other by the fibers.

[0012] When a continuous temperature gradient is given between the inner and outer surfaces of the PTFE tube upon the sintering in such a manner that the temperature of the outer surface is higher than that of the inner surface by 50-300°C, the fiber-knot structure is rearranged from the inner surface of the tube to the outer surface, so that portions whose fibers are more stretched than those before the treatment and hence made longer, and portions whose fiber are made shorter than those before the treatment are obtained.

[0013] Besides, when portions of the PTFE tube after the stretching are heated further at a temperature of 327°C or higher in accordance with the process described in Japanese patent Publication No. 1656/1983 or Japanese Patent Application Laid-Open No. 76648/1980, a tubular PTFE porous body excellent in strength in the direction perpendicular to the stretching direction can be produced.

Tube, fiber and sheet combined with antibacterial substance

[0014] The tube, fiber or sheet combined with the antibacterial substance can be produced by (1) a process in which an antibacterial substance is mixed and dispersed in a polymeric material, and the resulting mixture is formed into a tube, fiber or sheet, (2) a process in which an antibacterial substance is impregnated into and/or deposited on a porous tube, fiber or sheet formed

from a polymeric material, (3) a process in which a mixture of a biodegradable polymer and an antibacterial substance is impregnated into and/or deposited on a porous tube, fiber or sheet formed from a polymeric material, or the like.

[0015] In the process in which the mixture of the polymeric material and the antibacterial substance is formed into the tube, fiber or sheet, the tube, fiber or sheet may preferably be made porous.

[0016] In the process in which the antibacterial substance or the mixture of the biodegradable polymer and the antibacterial substance is impregnated into and/or deposited on the porous tube, fiber or sheet formed from the polymeric material, the antibacterial substance or the mixture of the biodegradable polymer and the antibacterial substance is impregnated into and/or deposited on the inner and outer surfaces of the porous tube, the outer surface of the porous fiber, the outer surface of the porous sheet and the inner surfaces defining pores in these porous bodies. The impregnation and/or deposition may be performed to the whole or parts of the pores, inner surface and outer surface of the porous tube, fiber or sheet. The antibacterial substance or the mixture of the biodegradable polymer and the antibacterial substance may be only impregnated into the pores in the porous body and deposited on the inner surfaces defining the pores in the porous body. In this invention, the term "impregnation" means that the antibacterial substance or the mixture of the biodegradable polymer and the antibacterial substance is impregnated into void spaces (i.e., pores) in the porous body to hold it therein. On the other hand, the term "deposition" means that the antibacterial substance or the mixture of the biodegradable polymer and the antibacterial substance is deposited on the inner surface (in the case of the porous tube) and outer surface of the porous body and the inner surfaces defining the pores in the porous body. In fact, both impregnation and deposition often take place.

[0017] Examples of the polymeric material from which the porous tube, fiber or sheet is formed may include synthetic polymeric materials such as polytetrafluoroethylene, tetrafluoroethylene-hexafluoropropylene copolymers, polyester, polyurethane, polyethylene and polypropylene. Besides, as the polymeric material, may be used biodegradable polymers (biotransformable polymers) such as agarose, dextran, polylactic acid, gelatin, fibrinogen, chitin and chitosan.

[0018] No particular limitation is imposed on the process for producing the porous tubes, fibers or sheets from these synthetic resin materials. For example, in the case where PTFE is used as a polymeric material, a porous tube may be produced in the same manner as in the tubular PTFE porous body in the vascular prosthesis described above. Following the process described in Japanese Patent Publication No. 18977/1990, PTFE containing a liquid lubricant may be formed into a fine rod. After removing the liquid lubricant, the rod may be stretched in its longitudinal direction into a porous fiber.

Alternatively, a porous sheet may be produced in accordance with the process described in Japanese Patent Publication No. 3842/1985. Similarly, a porous tube may be formed by producing a porous thin-film material composed of PTFE in advance, winding the thin-film material on a metallic wire to fix it and then integrally sintering the thin-film material under heat.

[0019] No particular limitation is also imposed on the process for producing the porous tubes, fibers or sheets from the biodegradable polymers. Examples thereof may include (1) a process for producing a tube composed of a biodegradable polymer, in which a solution of the biodegradable polymer is coated on the outer wall surface of a tube made of a suitable material to dry the polymer, and the tube situated inside the biodegradable polymer is then drawn out in this state, (2) a process for forming a fiber, in which a solution of a biodegradable polymer is filled into the bore of a tube made of a suitable material to dry the polymer, and the dried polymer is then drawn out of the tube, and (3) a process in which a solution of a biodegradable polymer is spread on a flat plate made of a suitable material, and the polymer is then dried.

[0020] In the process for producing the tube, fiber or sheet from the mixture of the polymeric material and the antibacterial substance, it is preferable that the biodegradable polymer be used as the polymeric material. In this case, when a mixed solution obtained by mixing a solution of the biodegradable polymer and the antibacterial substance in advance is used in the above-described production process of the tube, fiber or sheet composed of the biodegradable polymer, the antibacterial substance can be evenly dispersed in the biodegradable polymer, whereby the antibacterial substance can be dispersed and fixed in the biodegradable polymer in the form of a tube, fiber or sheet after drying the polymer. The antibacterial substance may bond to the biodegradable polymer by ionic bonding. As a solvent, there is generally used an organic solvent which does not decompose the biodegradable polymer and antibacterial substance. The tube, fiber or sheet composed of the biodegradable polymer is preferably made porous. The tube, fiber or sheet composed of the biodegradable polymer and combined with the antibacterial substance in accordance with this process can gradually release the antibacterial substance over a long period of time.

[0021] In the method of impregnating with and/or depositing the antibacterial substance into and/or on the porous tube, fiber or sheet formed from the polymeric material, it is only necessary to immerse the porous tube, fiber or sheet in a solution with the antibacterial substance dissolved therein and then dry the porous body. By this method, the antibacterial substance can be impregnated into and/or deposited on the whole or part of the pores, inner surface and outer surface of the porous body.

[0022] In order to control the release of the antibacterial substance over a long period of time, it is preferable

that a mixture of the biodegradable polymer and the antibacterial substance be impregnated into and/or deposited on the porous tube, fiber or sheet formed from the polymeric material. In this method, it is only necessary to immerse the porous tube, fiber or sheet in a mixed solution of the biodegradable polymer and the antibacterial substance and then dry the porous body. By this method, the antibacterial substance evenly dispersed in the biodegradable polymer can be impregnated into and/or deposited on the whole or part of the pores, inner surface and outer surface of the porous body. In this case, the above-mentioned various biodegradable polymers may be used as the biodegradable polymer. As a solvent, there is generally used a volatile organic solvent which can enter void spaces in the porous body and does not decompose the biodegradable polymer and antibacterial substance.

[0023] As the antibacterial substance, may be used antibiotics such as  $\beta$ -lactam, aminoglycoside, chloramphenicol, tetracycline, macrolide and lincomycin and heavy metals such as silver compounds. These substances may be used either singly or in any combination thereof.

[0024] The tube, fiber or sheet combined with the antibacterial substance is wound on the outer surface of the vascular prosthesis. However, it is wound with a desired space, not on the whole outer surface, so that the porous structure of the vascular prosthesis is not impaired. It is desirable that the outer diameter (size) of the tube or fiber combined with the antibacterial substance, or the thickness and width of the sheet combined with the antibacterial substance be smaller than the outer diameter of the vascular prosthesis, for example, about a half or smaller, preferably about a third or smaller, more preferably about a fourth or smaller of the outer diameter of the vascular prosthesis.

[0025] The release rate of the antibacterial substance is basically determined by the diffusion rate in the humor in which the antibacterial substance exudes after the implantation of the antibacterial vascular prosthesis according to the present invention. However, it may be controlled by selecting the pore size, porosity, wall thickness, size or width of the porous tube, fiber or sheet combined with the antibacterial substance, the kind of the biodegradable polymer, the compositional ratio of the biodegradable polymer to the antibacterial substance, the bonding between the biodegradable polymer and the antibacterial substance, the winding pitch on the vascular prosthesis of the tube, fiber or sheet, or the like. The combined amount of the antibacterial substance can be suitably determined. According to the present invention, however, it is possible to combine the antibacterial substance in a comparatively great amount compared with the conventional methods in which the antibacterial substance is bonded to the vascular prosthesis itself because the antibacterial substance is combined with the tube, fiber or sheet composed of the polymeric material. It is therefore possible to combine the

antibacterial substance in an amount sufficient to gradually release it until an immune system normally operates *in vivo* after the implantation of the vascular prosthesis. The amount can be experimentally determined from the kind and release rate of the antibacterial substance, and the like by those skilled in the art.

[0026] Since the antibacterial substance and the tube, fiber or sheet combined with the antibacterial substance exist only on the outer surface of the vascular prosthesis, they do not directly contact with the blood stream. Therefore, the innate antithrombogenicity in the vascular prosthesis is not impaired. According to the antibacterial vascular prosthesis of the present invention, the antibacterial substance released exists only on the outer surface of the vascular prosthesis or in its wall in the vicinity of the outer surface. Therefore, the histocompatibility of the vascular prosthesis is not impaired. Besides, since the porous structure of the vascular prosthesis is maintained, the penetrability of living tissues through the vascular prosthesis is kept good, and so the healing process is also not inhibited.

[0027] After the implantation of the antibacterial vascular prosthesis according to the present invention, the antibacterial substance is released near the outer surface of the vascular prosthesis. In this case, the antibacterial substance is gradually released over a long period of time owing to such that a sufficient amount of the antibacterial substance can be combined with the tube, fiber or sheet, and that such a combination of the antibacterial substance permits the control of release rate. The gradual release of the antibacterial substance allows the antibacterial substance to inhibit the growth of bacteria attached to the outer surface of the main vascular prosthesis over a long period of time. Meanwhile, the innate immune system in the living body comes to fully operate, and the tissues penetrate into the main vascular prosthesis, so that the healing is caused to progress.

[0028] The tube or fiber according to the present invention, which has been formed from the polymeric material and combined with the antibacterial substance, is also useful in applying to a surgical suture by itself. An incision site upon surgery has the highest possibility of being the source of infection. However, the use of the surgical suture composed of the tube or fiber combined with the antibacterial substance in such a site permits inhibiting the growth of the bacteria attached to the incision site as the source of infection over a long period of time because the antibacterial substance is gradually released over a long period of time.

#### ADVANTAGES OF THE INVENTION

[0029] According to the present invention, there is provided an antibacterial vascular prosthesis capable of exhibiting an antibacterial activity over a long period of time without impairing the porous structure, antithrombogenicity and histocompatibility inherent in a vascular prosthesis composed of a tubular porous body formed

of a synthetic polymer.

[0030] The present invention also provides an antibacterial surgical suture capable of exhibiting an antibacterial activity over a long period of time.

#### EMBODIMENTS OF THE INVENTION

[0031] The present invention will hereinafter be described more specifically by the following examples. However, it should be borne in mind that this invention is not limited to and by these examples only.

#### Example 1:

[0032] One gram of ofloxacin (antibiotic, product of Daiich Seiyaku Co., Ltd.) was suspended in 10 ml of a 1% solution of polylactic acid (molecular weight: 50,000, product of Polyscience Co.) in dioxane (product of Wako Pure Chemical Industries, Ltd.) which had been prepared in advance.

[0033] After a tape obtained by cutting a porous PTFE sheet (LUP-300, product of Sumitomo Electric Industries, Ltd.) into a width of 5 mm was spirally wound at the pitch of 2.5 mm on a stainless steel rod 1 mm in outer diameter, both ends of the tape were fixed to the rod, followed by heating of the tape at a temperature not lower than the melting point of PTFE to integrally sinter the tape, thereby forming the tape in the form of a tube. The stainless steel rod was then drawn out of the tube.

[0034] The porous PTFE tube thus obtained was immersed in the above-prepared mixed solution of ofloxacin and polylactic acid in dioxane to sufficiently penetrate the solution into the wall of the porous body. The thus-treated tube was then air-dried. This procedure was repeated 3 times, whereby the mixture of polylactic acid and ofloxacin was impregnated into the wall and deposited on the inner surface of the tube to obtain a composite tube.

[0035] The thus-obtained tube combined with ofloxacin and polylactic acid was lightly immersed in a 1% solution of polylactic acid in dioxane to wash out polylactic acid and ofloxacin present on the outer surface of the tube and at the same time, soften the tube as a whole. Thereafter, the tube was wound at a pitch of 5 mm on a stretched PTFE vascular prosthesis (Technograft, product of Sumitomo Electric Industries, Ltd.) 4 mm across and 5 cm long and then air-dried.

[0036] Both ends of the thus-obtained antibacterial vascular prosthesis were separately connected to a silicone tube, and a PBS solution (phosphate buffered-saline solution) was caused to flow at a rate of 10 ml/min through the bore of the tube by a peristaltic pump. At the same time, only the part of the vascular prosthesis was immersed in the same PBS solution as described above in a beaker to determine whether ofloxacin was dissolved out of the inner surface and outer surface of the vascular prosthesis by the measurement of absorbance at 280 nm of the PBS solution. As a result, no dissolving-

out of ofloxacin from the inner surface of the vascular prosthesis was detected. As illustrated in FIG. 1, however, ofloxacin was gradually being released from the outer surface of the vascular prosthesis even after 48 hours.

[0037] The antibacterial activity against *Escherichia coli* (JM109) of the antibacterial vascular prosthesis obtained above was evaluated. On an agar LB medium (1% bactotryptone, 0.5% yeast extract, 0.5% common salt, 1.5% agar) on a plate 10 cm across, were spread  $10^4$  cells of *Escherichia coli*. The antibacterial vascular prosthesis 1 cm long was left at rest in the center of the medium, and the cells were then cultured at 37°C for 18 hours. As a result, no proliferation of *Escherichia coli* was observed within a radius of 22 mm from the antibacterial vascular prosthesis. It was hence confirmed that the antibacterial vascular prosthesis according to the present invention has excellent antibacterial activity.

#### Example 2:

[0038] A tube combined with ofloxacin and polylactic acid, which had been produced in the same manner as in Example 1, was wound 75 mm in length on a stretched PTFE vascular prosthesis (Technograft) 4 mm across and 5 cm long. The thus-obtained composite vascular prosthesis was implanted under the back skin of a rabbit (New Zealand White, male). After a week, the back was incised to take the prosthesis sample out of the back. The sample was evaluated in the antibacterial activity against *Escherichia coli* (JM109) in the same manner as in Example 1. As a result, no proliferation of *Escherichia coli* was observed within a radius of 17 mm from the sample. It was hence confirmed that the antibacterial vascular prosthesis according to the present invention has excellent antibacterial activity even in the living body.

#### Claims

1. A vascular prosthesis comprising a tubular porous body formed of a synthetic polymer and, wound around the body, a tube, fibre or sheet formed from a polymeric material and combined with an antibacterial substance, wherein the outer surface of the body is partially uncovered and the porosity of the prosthesis relative to that of the body is unimpaired.
2. A prosthesis according to claim 1, wherein the polymeric material is porous.
3. A prosthesis according to claim 1 or claim 2, wherein the polymeric material is polytetrafluoroethylene or a tetrafluoroethylene-hexafluoropropylene copolymer.
4. A prosthesis according to any preceding claim,

wherein the polymeric material is or includes a biodegradable polymer.

5. A prosthesis according to claim 4, wherein the biodegradable polymer is selected from agarose, dextran, polylactic acid, gelatin, fibrinogen, chitin and chitosan.
6. A prosthesis according to any preceding claim, wherein the synthetic polymer is polytetrafluoroethylene.
7. A prosthesis according to any preceding claim, wherein the antibacterial substance is an antibiotic or a heavy metal.
8. A prosthesis according to claim 7, wherein the antibacterial substance is a  $\beta$ -lactam, aminoglycoside, chloramphenicol, tetracycline, macrolide, lincosamin or a silver compound.
9. A prosthesis according to any preceding claim, which includes a space between the tube, fibre or sheet and the outer surface of the body.
10. A prosthesis according to any preceding claim, wherein the outer diameter, size or thickness and width of the tube, fibre or sheet respectively, combined with the antibacterial substance, is/are smaller, e.g. 50% or less, than the outer diameter of the body.

#### Patentansprüche

1. Gefäßprothese, umfassend einen aus einem synthetischen Polymer gebildeten schlauchförmigen porösen Körper und, um den Körper gewunden, einen Schlauch, eine Faser oder Folie, gebildet aus einem polymeren Material und kombiniert mit einer antibakteriellen Substanz, wobei die äußere Oberfläche des Körpers teilweise unbedeckt ist und die Porosität der Prothese im Vergleich zu derjenigen des Körpers unbeeinträchtigt ist.
2. Prothese nach Anspruch 1, wobei das polymere Material porös ist.
3. Prothese nach Anspruch 1 oder Anspruch 2, wobei das polymere Material Polytetrafluorethylen oder ein Tetrafluorethylen-Hexafluorpropylen-Copolymer ist.
4. Prothese nach irgendeinem der vorhergehenden Ansprüche, wobei das polymere Material ein biologisch abbaubares Polymer ist oder einschließt.
5. Prothese nach Anspruch 4, wobei das biologisch

- abbaubare Polymer aus Agarose, Dextran, Polymilchsäure, Gelatine, Fibrinogen, Chitin und Chitosan ausgewählt ist.
6. Prothese nach irgendeinem der vorhergehenden Ansprüche, wobei das synthetische Polymer Polytetrafluorethylen ist. 5
7. Prothese nach irgendeinem der vorhergehenden Ansprüche, wobei die antibakterielle Substanz ein Antibiotikum oder ein Schwermetall ist. 10
8. Prothese nach Anspruch 7, wobei die antibakterielle Substanz ein  $\beta$ -Lactam, Aminoglycosid, Chloramphenicol, Tetracyclin, Macrolid, Lincomycin oder eine Silber-Verbindung ist. 15
9. Prothese nach irgendeinem der vorangehenden Ansprüche, welche einen Abstand zwischen dem Schlauch, der Faser oder Folie und der äußeren Oberfläche des Körpers einschließt. 20
10. Prothese nach irgendeinem der vorhergehenden Ansprüche, wobei der Außendurchmesser, die Größe oder Dicke und Breite des Schlauchs, der Faser bzw. Folie, kombiniert mit der antibakteriellen Substanz; kleiner, z.B. 50% oder weniger, als der Außendurchmesser des Körpers ist/sind. 25
6. Prothese selon l'une quelconque des revendications précédentes, où le polymère synthétique est le polytétrafluoroéthylène.
7. Prothese selon l'une quelconque des revendications précédentes, où la substance antibactérienne est un antibiotique ou un métal lourd. 5
8. Prothese selon la revendication 7, où la substance antibactérienne est un  $\beta$ -lactame, un aminoglycoside, le chloramphénicol, une tétracycline, un macrolide, la lincomycine ou un composé de l'argent. 10
9. Prothese selon l'une quelconque des revendications précédentes qui comprend un espace entre le tube, la fibre ou la feuille et la surface externe du corps. 15
10. Prothese selon l'une quelconque des revendications précédentes, où le diamètre externe, la taille ou l'épaisseur et la largeur du tube, de la fibre ou de la feuille, respectivement, combiné avec la substance antibactérienne, est/sont inférieur(s), par exemple de 50 % ou moins, au diamètre externe du corps. 20

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#### Revendications

1. Prothese vasculaire comprenant un corps poreux tubulaire constitué par un polymère synthétique et, enroulé autour du corps, un tube, une fibre ou une feuille en une matière polymère et combiné avec une substance antibactérienne, où la surface externe du corps est partiellement non recouverte et la porosité de la prothèse n'est pas détériorée par rapport à celle du corps. 35
2. Prothese selon la revendication 1, où la matière polymère est poreuse. 40
3. Prothese selon la revendication 1 ou la revendication 2, où la matière polymère est le polytétrafluoroéthylène ou un copolymère tétrafluoroéthylène-hexafluoropropylène. 45
4. Prothese selon l'une quelconque des revendications précédentes, où la matière polymère est ou inclut un polymère biodégradable. 50
5. Prothese selon la revendication 4, où le polymère biodégradable est choisi parmi l'agarose, le dextrane, le poly(acide lactique), la gélatine, le fibrinogène, la chitine et le chitosane. 55

FIG. 1

